Research Article

Escalation with Overdose Control Using Ordinal Toxicity Grades for Cancer Phase I Clinical Trials

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We extend a Bayesian adaptive phase I clinical trial design known as escalation with overdose control (EWOC) by introducing an intermediate grade 2 toxicity when assessing dose-limiting toxicity (DLT). Under the proportional odds model assumption of dose-toxicity relationship, we prove that in the absence of DLT, the dose allocated to the next patient given that the previously treated patient had a maximum of grade 2 toxicity is lower than the dose given to the next patient had the previously treated patient exhibited a grade 0 or 1 toxicity at the most. Further, we prove that the coherence properties of EWOC are preserved. Simulation results show that the safety of the trial is not compromised and the efficiency of the estimate of the maximum tolerated dose (MTD) is maintained relative to EWOC treating DLT as a binary outcome and that fewer patients are overdosed using this design when the true MTD is close to the minimum dose.

1. Introduction

Cancer phase I clinical trials are sequential designs enrolling late stage cancer patients who have exhausted standard treatment therapies [1]. For cytotoxic agents or combinations of biologic with cytotoxic drugs, the main objectives of these trials are to characterize treatment-related toxicities and estimate a dose level that is associated with a predetermined level of dose limiting toxicity (DLT). Such a dose is called maximum tolerated dose (MTD) or phase II dose. Specifically, the MTD, γ , is defined as the dose that is expected to produce DLT after one cycle of therapy in a specified proportion θ of patients:

$$P(\text{DLT} \mid \text{Dose} = \gamma) = \theta. \tag{1.1}$$

Although the definition of DLT depends on the cancer type and the agent under study, it is typically defined as a grade 3 or 4 nonhematologic and grade 4 hematologic toxicity for

cytotoxic agents, see the National Cancer Institute (NCI) common toxicity criteria [2]. The value chosen for the target probability of DLT θ depends on the nature and severity of the DLT; it is set relatively high when the DLT is a transient, reversible, and nonfatal condition and low when it is lethal or life threatening.

Model-based designs for cancer phase I clinical trials have been studied extensively in the last two decades; see O'Quigley et al. [3], Gatsonis and Greenhouse [4], Durham and Flournoy [5], Korn et al. [6], Whitehead and Brunier [7], Whitehead [8], Babb et al. [9], Gasparini and Eisele [10], Mukhopadhyay [11], and Haines et al. [12]. In particular, the continual reassessment method (CRM) first proposed by O'Quigley et al. [3] is Bayesian outcome adaptive, and has been modified and extended by many authors; see, for example, Faries [13], Moller [14], Goodman et al. [15], O'Quigley and Shen [16], Piantadosi et al. [17], Cheung and Chappell [18], Storer [19], and Leung and Wang [20]. The attribute of the CRM is that at each stage of the trial, we seek a dose for which a Bayes estimate of the probability of DLT is closest to the target probability of DLT θ . Escalation with overdose control (EWOC) originally proposed by Babb et al. [9] is another alternative Bayesian outcome adaptive design for dose finding in early phase cancer trials. Unlike CRM, its main feature is that at each stage of the trial, we seek a dose for which the posterior probability of exceeding the MTD γ is bounded by a feasibility bound α . Statistical properties of EWOC have been studied by Zacks et al. [21], Tighiouart et al. [22], and Tighiouart and Rogatko [23], and examples of phase I trials using EWOC can be found in [24–33]. Further literature review of statistical methods for dose finding in cancer phase I trials can be found in Ting [34] and Chevret [35].

The above methods allocate future doses based on a binary outcome of DLT of previously treated patients. Such designs may not be efficient in the sense that the dose recommended for the next patient is the same regardless whether the previously treated patient had no toxicity or had an intermediate grade 2 toxicity. The work we present in this manuscript is motivated by the ethical concern raised by clinical colleagues regarding dose escalation in the absence of DLT. Specifically, if the current patient experiences drug related grade 2 toxicity at the most, then the dose to be allocated to the next patient should not be as high as the one had the current patient experienced a maximum of grade 0 or 1 toxicity. We present a Bayesian outcome adaptive design which is an extension of EWOC by accommodating an intermediate grade 2 toxicity to the model. We use a proportional odds model to describe the dose-toxicities relationship and the design is termed EWOC proportional odds model, written as EWOC-POM. We show that the design satisfies the above ethical consideration without compromising the safety and efficiency of the trial. Furthermore, we show that the design maintains the coherence properties of EWOC.

Cancer phase I clinical trials designs taking into account all grades and types of toxicities have been proposed by many authors with the goal of improving the safety and efficiency of the trial, see Gordon and Willson [36], Wang et al. [37], Bekele and Thall [38], Yuan et al. [39], Potthoff and George [40], Bekele et al. [41], Van Meter et al. [42, 43], Iasonos et al. [44], Lee et al. [45], and Chen et al. [46]. Some of these methods use multivariate models for characterizing the different grades of toxicities as a function of dose while others summarize the information from all toxicity grades into a continuous score. Depending on the underlying scenarios, in general, adding multiple toxicity grades information to the model has little effect on the safety of the trial with a modest gain in the precision of the estimate of the MTD. Our contribution in this manuscript is motivated by the ethical constraint that dose escalation in the absence of DLT should be mitigated by the occurrence of an intermediate grade 2 toxicity. The model and design we propose is constructed in such a way as to maintain the main

properties of EWOC while at the same time, satisfying those ethical considerations raised by our clinical colleagues.

The manuscript is organized as follows. In Section 2, we give a detailed description of the methodology and describe the trial design. In Section 3, we state and prove the ethical considerations and coherence properties of EWOC-POM. The simulation results of the design operating characteristics and comparison with EWOC design are included in Section 4. Section 5 contains some final remarks and discussion of practical implementations.

2. Method

2.1. Model

Let G = 0, 1, ..., 4 be the maximum grade of toxicity experienced by a patient by the end of one cycle of therapy and define DLT as a maximum of grade 3 or 4 toxicity. Let

$$Y = \begin{cases} 0 & \text{if } G = 0 \text{ or } 1 \\ 1 & \text{if } G = 2 \\ 2 & \text{if } G = 3 \text{ or } 4. \end{cases}$$
(2.1)

We model the dose-toxicities relationship by assuming that

$$P(Y \ge j \mid x) = F(\alpha_j + \beta x), \quad j = 1, 2,$$

$$(2.2)$$

where $F(\cdot)$ is a known strictly increasing cdf. This implies that $\alpha_2 \le \alpha_1$. We assume that $\beta > 0$ so that the probability of DLT is an increasing function of dose. The MTD, γ , is defined as the dose that is expected to produce DLT in a specified proportion θ of patients:

$$P(Y = 2 \mid x = \gamma) = F(\alpha_2 + \beta\gamma) = \theta.$$
(2.3)

The value chosen for the target probability θ depends on the nature and clinical manageability of the DLT; it is set relatively high when the DLT is a transient, correctable, or nonfatal condition and low when it is lethal or life threatening. Suppose that dose levels in the trial are selected in the interval [X_{min}, X_{max}].

2.1.1. Likelihood

Let $D_n = \{(x_i, Y_i), i = 1, ..., n\}$ be the data after enrolling *n* patients to the trial. The likelihood function for the parameters α_1 , α_2 , and β is

$$L(\alpha_{1}, \alpha_{2}, \beta \mid D_{n}) = \prod_{i=1}^{n} \left[1 - F(\alpha_{1} + \beta x_{i})\right]^{I(Y_{i}=0)} \left[F(\alpha_{1} + \beta x_{i}) - F(\alpha_{2} + \beta x_{i})\right]^{I(Y_{i}=1)} \times \left[F(\alpha_{2} + \beta x_{i})\right]^{I(Y_{i}=2)},$$
(2.4)

where $I(\cdot)$ is the indicator function.

We reparameterize model (2.2) in terms of $\rho_0 = P(Y = 2 | x = X_{\min})$, the probability that a DLT manifests within the first cycle of therapy for a patient given dose $x = X_{\min}$, $\rho_1 = P(Y \ge 1 | x = X_{\min})$, the probability that a grade 2 or more toxicity manifests within the first cycle of therapy for a patient given dose $x = X_{\min}$, and the MTD γ . This reparameterization is convenient to clinicians since γ is the parameter of interest. Assuming that the dose is standardized to be in the interval [0, 1], it can be shown that

$$\alpha_{1} = F^{-1}(\rho_{1}), \qquad \alpha_{2} = F^{-1}(\rho_{0}),$$

$$\beta = \frac{1}{\gamma} \Big(F^{-1}(\theta) - F^{-1}(\rho_{0}) \Big).$$
(2.5)

The conditions $\alpha_2 \leq \alpha_1$, $\beta > 0$, and (2.2) imply that $0 \leq \rho_0 \leq \rho_1$ and $0 \leq \rho_0 \leq \theta$. Define

$$F_{1}(\rho_{0},\rho_{1},\gamma;x) = F\left(F^{-1}(\rho_{1}) + \left(F^{-1}(\theta) - F^{-1}(\rho_{0})\right)\frac{x}{\gamma}\right)$$

$$F_{2}(\rho_{0},\rho_{1},\gamma;x) = F\left(F^{-1}(\rho_{0}) + \left(F^{-1}(\theta) - F^{-1}(\rho_{0})\right)\frac{x}{\gamma}\right).$$
(2.6)

Using (2.4), (2.5), and (2.6), the likelihood of the reparameterized model is

$$L(\rho_{0},\rho_{1},\gamma \mid D_{n}) = \prod_{i=1}^{n} \left[1 - F_{1}(\rho_{0},\rho_{1},\gamma;x_{i})\right]^{I(Y_{i}=0)} \left[F_{1}(\rho_{0},\rho_{1},\gamma;x_{i}) - F_{2}(\rho_{0},\rho_{1},\gamma;x_{i})\right]^{I(Y_{i}=1)} \times \left[F_{2}(\rho_{0},\rho_{1},\gamma;x_{i})\right]^{I(Y_{i}=2)}.$$
(2.7)

2.1.2. Prior and Posterior Distributions

Let $g(\rho_0, \rho_1, \gamma)$ be the prior distribution on Ω , where $\Omega = \{(x, y, z) : 0 \le x \le \theta, x \le y \le 1, X_{\min} \le z \le X_{\max}\}$. Using Bayes rule, the posterior distribution of the model parameters is proportional to the product of the likelihood and prior distribution

$$\pi(\rho_0, \rho_1, y \mid D_n) \propto L(\rho_0, \rho_1, \gamma \mid D_n) \times g(\rho_0, \rho_1, \gamma).$$

$$(2.8)$$

We designed an MCMC sampler based on the Metropolis-Hastings algorithm [47, 48] to obtain model operating characteristics. We also used WinBUGS [49] to estimate features of the posterior distribution of the MTD and design a trial. The WinBUGS code is included in the Appendix section. In the absence of prior information about the MTD and probability of DLT at X_{min} , we specify vague priors for the model parameters as follows:

$$\gamma \sim \text{Unif}[X_{\min}, X_{\max}]$$

$$\rho_0 \sim \text{Unif}[0, \theta]$$

$$\rho_1 \mid \rho_0 \sim \text{Unif}[\rho_0, 1].$$
(2.9)

2.1.3. Trial Design

Dose levels in the trial are selected in the interval $[X_{\min}, X_{\max}]$. The adaptive design proceeds as follows. The first patient receives a dose $x_1 > X_{\min}$ that is deemed to be safe by the clinician. Denote by $\Pi k(\gamma) = \Pi(\gamma \mid D_k)$ the marginal posterior cdf of the MTD, k = 1, ..., n - 1. The (k+1)-st patient receives the dose $x_{k+1} = \Pi_k^{-1}(\alpha)$ so that the posterior probability of exceeding the MTD is equal to the feasibility bound α . This is the overdose protection property of EWOC, where at each stage of the design, we seek a dose to allocate to the next patient while controlling the posterior probability of exposing patients to toxic dose levels. The trial proceeds until a predetermined number of n patients are enrolled to the trial. At the end of the trial, we estimate the MTD as $\hat{\gamma} = \Pi_n^{-1}(\alpha)$.

3. Properties of EWOC-POM

3.1. Characteristics of EWOC-POM

The proposed design EWOC-POM assigns dose levels to future patients by taking into account the maximum observed toxicity grade during the first cycle of therapy according to the following properties.

- (i) At each stage of the design, we seek a dose to allocate to the next patient while controlling the posterior probability of exposing patients to toxic dose levels.
- (ii) If the maximum grade of toxicity experienced by patient *k* − 1 within one cycle of therapy is grade 2, then the dose allocated to patient *k* is lower than the dose that would have been given to patient *k* had the maximum grade of toxicity experienced by patient *k* − 1 been grade 0 or 1.

Property (i) is the overdose protection defining characteristic of EWOC which is also satisfied by EWOC-POM. Property (ii) is naturally appealing because when a patient experiences grade 2 dose-related toxicity, then it is ethical not to increase the dose by the same amount had this patient exhibited grade 0 or 1 toxicity at the most. Characteristic (ii) is summarized in the following theorem.

Theorem 3.1. Let $D_k = \{(Y_1, x_1), \dots, (Y_k, x_k)\}$ be the data on the first k patients generated by the design described in Section 2.1.3, and, $\Pi_k(\gamma; Y_k)$ be the cdf of γ given the data D_k . Let $x_{k+1} = \Pi_k^{-1}(\alpha; Y_k)$ and $x'_{k+1} = \Pi_k^{-1}(\alpha; Y'_k)$. Suppose that for all $x \in [X_{\min}, X_{\max}]$ and all (ρ_0, ρ_1) such that $0 \le \rho_0 \le \rho_1 \le 1$ and $\rho_0 \le \theta$, $(F_1 - F_2)/(1 - F_1)$ is a monotonically decreasing function in γ . Then, $x'_{k+1} \ge x_{k+1}$ whenever $Y'_k = 0$ and $Y'_k = 1$.

The proof of Theorem 3.1 is given in the Appendix section. It is easy to verify that the monotonicity condition of Theorem 3.1 holds for the logistic function $F(w) = 1/(1 + e^{-w})$. Using this link function and the uniform priors given in (2.9) with $\theta = 0.33$, Figure 1 gives all possible dose assignments for patients 1 and 2 and selected situations for patients 3 and 4 using the trial design described in Section 2.1.3. The dose has been standardized so that $X_{\min} = 0$ and $X_{\max} = 1$, and the first patient is given dose 0.10. If this patient experiences grade 0 or 1 toxicity at the most, the dose recommended for patient 2 is 0.36. On the other hand, if patient 1 experiences grade 2 toxicity at the most, the dose recommended for patient 2 is 0.22, much lower than 0.36. This figure also illustrates some of the coherence properties stated in Theorem 3.2 below.



Figure 1: Tree of possible dose allocations for patients 1 and 2 and selected situations for patients 3 and 4. G = 0, 1 corresponds to Y = 0, G = 2 corresponds to Y = 1, and G = 3, 4 corresponds to Y = 2 or DLT.

3.2. Coherence of EWOC-POM

In cancer phase I clinical trials, it is ethical not to increase a dose of a cytotoxic agent for the next patient if the previously treated patient exhibited DLT when given the same dose level. Furthermore, it is desirable not to decrease the dose of an agent for the next patient if the previously treated patient did not experience DLT when given that same dose level. These two properties are known as coherence in escalation and de-escalation, respectively, see Cheung [50]. A design that satisfies both of these properties is said to be coherent. Tighiouart and Rogatko [23] show that EWOC is coherent. The next theorem states some of the coherence properties of EWOC-POM.

Theorem 3.2. Suppose that for all $x \in [X_{\min}, X_{\max}]$ and all (ρ_0, ρ_1) such that $0 \le \rho_0 \le \rho_1 \le 1$ and $\rho_0 \le \theta$, F_1 and F_2 are monotonically decreasing in γ . Then the design EWOC-POM described in 2.1.3 is coherent in deescalation. Furthermore, if the toxicity response for patient k is $Y_k = 0$, then the dose allocated to patient k + 1 satisfies $x_{k+1} \ge x_k$.

The proof of Theorem 3.2 is given in the Appendix section.

4. Simulation Studies

We compare the design operating characteristics of EWOC-POM with the original EWOC by simulating a large number of trials under several scenarios. We used the logistic function $F(w) = 1/(1+e^{-w})$ to model the dose-toxicities relationship in (2.2). EWOC was implemented as in Tighiouart et al. [22] using the same logistic function to model the dose-toxicity relationship. For all scenarios, we standardize the dose to be in the interval [0, 1], $\theta = 0.33$, the feasibility bound $\alpha = 0.25$, and the trial sample size is n = 30. The priors in (2.9) were adopted for EWOC-POM. We also carried out design operating characteristics for $\theta = 0.20$, and the conclusions regarding the performance of EWOC-POM relative to EWOC were essentially the same.

4.1. Algorithm

For a given scenario determined by ρ_0 , ρ_1 , and γ , the first patient receives dose 0, and the next dose x_2 is determined according to the trial design described in 2.1.3. The second



Figure 2: Dose-toxicity relationship for the nine scenarios considered in the design operations characteristics. The solid curves correspond to P(Y = 2 | x) = P(DLT | x) and the dashed curves in bold correspond to P(Y > 1 | x). The horizontal dashed lines represent the target probability of DLT θ = 0.33 and the vertical lines correspond to the true values of the MTD γ .

response y_2 is then generated from model (2.2) reparameterized in terms of ρ_0 , ρ_1 , and γ with $x = x_2$. This process is repeated until all n patients have been enrolled to the trial. We considered 9 scenarios corresponding to a fixed value for $\rho_0 = 0.05$, three values of ρ_1 , 0.2, 0.5, and 0.8, and three values of the MTD γ , 0.1, 0.5, and 0.7. The corresponding dose-toxicity relationships for these nine scenarios are illustrated in Figure 2. For each model and each scenario, we simulated M = 1000 trials. EWOC and EWOC-POM were compared in terms of the proportion of patients exhibiting DLT, the average bias, bias_{ave} = $M^{-1}(\sum_{i=1}^{M} \hat{\gamma}_i - \gamma_{true})$, and the estimated mean square error MSE = $M^{-1}(\sum_{i=1}^{M} (\hat{\gamma}_i - \gamma_{true})^2)$, where $\hat{\gamma}_i$ is the Bayes



Figure 3: Summary statistics for trial safety for EWOC and EWOC-POM under all scenarios. Each graph represents mean proportion obtained from all patients from all 1000 simulated trials.

		Percent of trial wi	th estimated	l MTD	Perc	ent of Trial
Scenarios	Within 0.05 of γ		Within 0.10 of γ		with rate of DLT >0.4	
	EWOC	EWOC-POM	EWOC	EWOC-POM	EWOC	EWOC-POM
$\gamma = 0.1, \rho_1 = 0.2$	98.3	98.4	100	100	7.5	6.6
$\gamma = 0.1, \rho_1 = 0.5$	98.3	97.5	100	100	7.5	3.0
$\gamma = 0.1, \rho_1 = 0.8$	98.3	96.4	100	100	7.5	2.9
$\gamma = 0.5, \rho_1 = 0.2$	39.6	40.5	70.3	71.3	0.2	0.0
$\gamma = 0.5, \rho_1 = 0.5$	39.6	35.6	70.3	63.2	0.2	0.0
$\gamma = 0.5, \rho_1 = 0.8$	39.6	31.0	70.3	59.4	0.2	0.0
$\gamma = 0.7, \rho_1 = 0.2$	24.3	27.6	49.1	53.3	0.0	0.0
$\gamma = 0.7, \rho_1 = 0.5$	24.3	23.2	49.1	45.7	0.0	0.0
$\gamma = 0.7, \rho_1 = 0.8$	24.3	20.1	49.1	37.1	0.0	0.0

Table 1: Percent of trials with estimated MTD within 5% of the dose range and 10% of the dose range of the true MTD γ and percent of trials for which the rate of DLT exceeds 40% for EWOC and EWOC-POM under the nine scenarios.

estimate of the posterior distribution of the MTD at the end of the *i*th trial with respect to the asymmetric loss function:

$$L(x,\gamma) = \begin{cases} \alpha(\gamma - x) & \text{if } x \le \gamma\\ (1 - \alpha)(x - \gamma) & \text{if } x > \gamma. \end{cases}$$
(4.1)

We also compared the models with respect to the proportion of patients that were overdosed. Here, a dose x is defined as an overdose if $x > x^*$, where x^* is defined as the dose for which $P(DLT | x^*) = \theta + 0.05$. This probability is calculated using the parameter values from the corresponding scenario. These models are further compared with respect to the proportion of patients that were overdosed given that the previously treated patient exhibited grade 2 toxicity. Finally, we compared EWOC-POM to EWOC in terms of the proportion of trials for which the probability of DLT exceeds 0.4. This gives us an estimate of the probability that a prospective trial will result in an excessively high DLT rate. As for the proportion of trials with correct MTD recommendation, we presented percent of trials with estimated MTD within 10% and 20% of the dose range of the true MTD for EWOC-POM and EWOC.

4.2. Results

Figure 3 shows that the proportion of patients exhibiting DLT is always less than 34% for both EWOC and EWOC-POM under all scenarios and 4% fewer patients experiencing DLT under EWOC-POM when the MTD is small ($\gamma = 0.1$) and $\rho_1 = 0.8$. The same figure shows that the proportion of patients that are overdosed using EWOC is uniformly higher relative to EWOC-POM when the MTD is small. The same trend is observed when $\gamma = 0.5$ except when $\rho_1 = 0.2$. The difference in the proportion of patients being overdosed when $\gamma = 0.7$ is negligible. The last panel of Figure 3 shows that the proportion of patients that are overdosed given that the previously treated patient exhibited grade 2 toxicity using EWOC is uniformly higher relative to EWOC-POM when $\gamma = 0.1$, 0.5 except when $\rho_1 = 0.2$. The difference in these proportions of Table 1 show that the precent of trials with DLT rate of 0.4 or more is 7.5% at the most for EWOC and 6.6% for EWOC-POM. A more detailed comparison is shown in Figure 4, where side-by-side box plots of



Figure 4: Box plots for the proportion of DLTs for EWOC-POM and EWOC under the nine scenarios. Each box plot was constructed from the DLT rates of the 1000 simulated trials. The dashed horizontal line corresponds to the target probability of DLT θ = 0.33.

the distributions of the proportion of DLTs for EWOC-POM and EWOC under the nine scenarios are displayed. These results show that EWOC-POM maintains the safety of the trial relative to EWOC and is much safer when the true MTD is close to the minimum dose by reducing the number of patients that are exposed to toxic doses.

Figure 5 shows that the estimated MTDs using EWOC and EWOC-POM are very close in general, with the highest difference observed when $\rho_1 = 0.8$. This is reflected by the estimated bias and RMSE shown in Figure 5. This is expected since EWOC-POM is characterized by a conservative dose escalation when a patient experiences grade 2 toxicity. The highest absolute value of the bias is 0.04 and is achieved when $\gamma = 0.5$, 0.7 and $\rho_1 = 0.8$. This constitutes 4% of the range of the dose and is practically not significant. The percent of trials with estimated MTD within 5% of the dose range and 10% of the dose range of the true MTD γ under the nine scenarios are shown in columns 2–5 of Table 1. These results further confirm that the precision of the estimate of the MTD is similar between the two models, with a higher precision for EWOC achieved when $\gamma = 0.5$ and $\rho_1 = 0.8$. Values other than 5% and 10% of the dose range were also used, and the conclusions were essentially the same. We conclude that EWOC-POM maintains the efficiency of the trial relative to EWOC for all practical purpose.

These simulation results suggest that EWOC-POM is a good alternative design for cancer phase I clinical trials which takes into account the ethical consideration that dose escalation in the absence of DLT is mitigated by the occurrence of a grade 2 toxicity.

4.3. Model Robustness

Model robustness with respect to assumption of proportional odds model in (2.2) was assessed by simulating the toxicity responses from a nonproportional odds model:

$$P(Y \ge j \mid x) = F(\alpha_j + \beta_j x), \quad j = 1, 2.$$
 (4.2)



Figure 5: Summary statistics for trial efficiency for EWOC and EWOC-POM under all scenarios. Each graph represents a mean value obtained from all patients from all 1000 trials.

The same logistic link function $F(w) = 1/(1 + e^{-w})$ was used. We considered two different models M₁ and M₂ corresponding to the set of parameters $\alpha_2 = -3.94$, $\beta_1 = 22.36$, $\beta_2 = 32.36$ for model M₁ and $\alpha_2 = -1.94$, $\beta_1 = 22.36$, $\beta_2 = 12.36$ for M₂. For each model M_i, *i* = 1, 2, we considered three different values for the intercept term α_1 , $\alpha_1 = -1.38$, 0.00, 1.38 which correspond to $\rho_1 = 0.2$, 0.5, 0.8. These parameters have been selected so that $\rho_0 = 0.020$ for



Figure 6: Dose-toxicity relationship under the proportional (EWOC-POM) and nonproportional odds models (M_1 and M_2) when the true MTD $\gamma = 0.1$. The dashed horizontal line corresponds to the target probability of DLT $\theta = 0.33$.

model M_1 , $\rho_0 = 0.126$ for model M_2 , and the true MTD is $\gamma = 0.1$. Figure 6 shows the graphs of the probabilities of DLT and probability of grade 2 or more toxicity as a function of dose for the proportional odds model POM and models M_1 and M_2 when $\rho_1 = 0.2$. For each scenario, we simulated 1000 trials with n = 30 patients where at each stage of the trial, the next dose is calculated using the trial design described in 2.1.3 as in Section 4.1 but the toxicity response is generated using the nonproportional odds model (4.2). The simulation results are summarized in Table 2. The maximum difference in proportion of patients exhibiting DLT (averaged across the simulated trials) between model M_i , i = 1, 2 and EWOC-POM is 3%. Under model M_2 , the proportion of patients that are overdosed is higher than EWOC-POM, and this proportion is 13% higher when $\rho_1 = 0.2$.

The percent of trials with DLT rate exceeding 0.4 is less than 15% in all cases. This percent is highest for model M_2 ; however, this is still relatively small compared to the results obtained in [42]. The percent of trials with estimated MTD within 10% of the dose range of the true MTD is 100% between the three models and across all scenarios and very good within 5% of the dose range of the true MTD.

In summary, EWOC-POM seems to be robust to model misspecification when the true MTD is near the initial dose. On the other hand, the model is sensitive to model misspecification when the true MTD is high but the safety of the trial is not compromised. We also conducted similar simulations (results not shown) when the true MTD is $\gamma = 0.5, 0.7$. We found that under all scenarios, the proportion of patients exhibiting DLT is always less than 33% but the bias tends to be higher for high values of ρ_1 and γ . This is the case when the probability of DLT curve increases very slowly as a function of dose which results in a very slow dose escalation scheme.

5. Discussion

In this paper, we proposed a Bayesian adaptive design for dose-finding studies in cancer phase I clinical trials. The method addresses the ethical concern regarding dose escalation in

Statistics	Model		$\begin{array}{c c c c c c c } & \rho_1 \\ \hline 0.2 & 0.5 \\ \hline 0.337 & 0.312 \\ \hline 0.328 & 0.304 \\ \hline 0.357 & 0.342 \\ \hline 0.274 & 0.155 \\ \hline 0.240 & 0.203 \\ \hline 0.274 & 0.203 \\ \hline 0.274 & 0.351 \\ \hline 0.093 & 0.090 \\ \hline 0.093 & 0.090 \\ \hline 0.094 & 0.092 \\ \hline 0.095 & 0.090 \\ \hline -0.007 & -0.010 \\ \hline -0.006 & -0.007 \\ \hline -0.005 & -0.010 \\ \hline -0.005 & -0.005 \\ \hline -0.005 & -0.010 \\ \hline -0.005 & -0.010 \\ \hline -0.0$	
Statistics	Widdei	0.2		0.8
	EWOC-POM	0.337	0.312	0.299
Proportion of DLTs	M_1	0.328	0.304	0.289
	M_2	0.357	0.342	0.331
	EWOC-POM	0.274	$\begin{array}{c} \rho_1 \\ 0.5 \\ 0.312 \\ 0.304 \\ 0.342 \\ 0.155 \\ 0.203 \\ 0.351 \\ 0.090 \\ 0.092 \\ 0.090 \\ -0.010 \\ -0.007 \\ -0.010 \\ 0.021 \\ 0.016 \\ 0.029 \\ 3.0 \\ 1.2 \\ 11.6 \\ 97.5 \\ 99.5 \\ 91.2 \\ 100.0 \\ 100.0 \\ 100.0 \\ 100.0 \\ 100.0 \\ 100.0 \\ \end{array}$	0.200
Proportion overdosed	M_1	0.240		0.173
	M_2	$\begin{array}{c cccc} & & \rho_1 \\ \hline 0.2 & 0.5 \\ \hline 0.337 & 0.312 \\ \hline 0.328 & 0.304 \\ \hline 0.357 & 0.342 \\ \hline 0.274 & 0.155 \\ \hline 0.240 & 0.203 \\ \hline 0.404 & 0.351 \\ \hline 0.093 & 0.090 \\ \hline 0.094 & 0.092 \\ \hline 0.095 & 0.090 \\ \hline -0.007 & -0.010 \\ \hline -0.006 & -0.007 \\ \hline -0.005 & -0.010 \\ \hline 0.022 & 0.021 \\ \hline 0.016 & 0.016 \\ \hline 0.027 & 0.029 \\ \hline 6.6 & 3.0 \\ \hline 1.5 & 1.2 \\ \hline 14.7 & 11.6 \\ \hline 98.4 & 97.5 \\ \hline 99.7 & 99.5 \\ \hline 91.1 & 91.2 \\ \hline 100.0 & 100.0 \\ \hline 100.0 & 100.0 \\ \hline 100.0 & 100.0 \\ \hline 0.020 & 0.001 \\ \hline \end{array}$	0.322	
	EWOC-POM	0.093	$\begin{array}{c} \rho_1 \\ 0.5 \\ 0.312 \\ 0.304 \\ 0.342 \\ 0.155 \\ 0.203 \\ 0.351 \\ 0.090 \\ 0.090 \\ 0.092 \\ 0.090 \\ 0.090 \\ 0.092 \\ 0.090 \\ 0.092 \\ 0.090 \\ 0.021 \\ 0.016 \\ 0.021 \\ 0.016 \\ 0.029 \\ 3.0 \\ 1.2 \\ 11.6 \\ 97.5 \\ 99.5 \\ 91.2 \\ 100.0 \\ 100.0 \\ 100.0 \\ 100.0 \\ 100.0 \\ 100.0 \\ 0.05 \\ 0$	0.087
MTD estimate	M_1	0.094	0.092	0.090
	M_2	0.095	0.090	0.086
	EWOC-POM	-0.007	-0.010	-0.013
Bias	M_1	-0.006	-0.007	-0.010
	M_2	-0.005	$\begin{array}{c} \rho_1 \\ 0.5 \\ 0.312 \\ 0.304 \\ 0.342 \\ 0.155 \\ 0.203 \\ 0.351 \\ 0.090 \\ 0.092 \\ 0.090 \\ -0.010 \\ -0.010 \\ -0.010 \\ 0.021 \\ 0.021 \\ 0.016 \\ 0.029 \\ 3.0 \\ 1.2 \\ 11.6 \\ 97.5 \\ 99.5 \\ 91.2 \\ 100.0 \\ 100.0 \\ 100.0 \\ 100.0 \\ 100.0 \\ 100.0 \\ 0.030 \\ 0.030 \\ 0.000 \\ $	-0.013
	EWOC-POM	0.022	0.021	0.023
Root MSE	M_1	0.016	0.016	0.017
	M_2	0.027	0.029	0.031
	EWOC-POM	6.6	3.0	2.9
Percent of trial with DLT rate >40%	M_1	1.5	1.2	0.8
	M_2	14.7	$\begin{array}{c} \rho_1 \\ 0.5 \\ \hline 0.312 \\ 0.304 \\ 0.342 \\ \hline 0.155 \\ 0.203 \\ 0.351 \\ \hline 0.090 \\ 0.092 \\ 0.090 \\ \hline -0.010 \\ \hline -0.010 \\ \hline -0.007 \\ \hline -0.010 \\ \hline 0.021 \\ 0.016 \\ 0.029 \\ \hline 3.0 \\ 1.2 \\ 11.6 \\ \hline 97.5 \\ 99.5 \\ 91.2 \\ \hline 100.0 \\ 100.0 \\ 100.0 \\ 100.0 \\ \hline 100.0 \\ \hline 0.012 \\ \hline$	12.6
	EWOC-POM	98.4	97.5	96.4
Percent of trial with estimated MTD within 0.05 of γ	M_1	99.7	$\begin{array}{c cccc} & \rho_1 \\ 2 & 0.5 \\ \hline 37 & 0.312 \\ \hline 28 & 0.304 \\ \hline 57 & 0.342 \\ \hline 74 & 0.155 \\ \hline 40 & 0.203 \\ \hline 04 & 0.351 \\ \hline 93 & 0.090 \\ \hline 94 & 0.092 \\ \hline 95 & 0.090 \\ \hline 007 & -0.010 \\ \hline 006 & -0.007 \\ \hline 006 & -0.007 \\ \hline 005 & -0.010 \\ \hline 22 & 0.021 \\ \hline 16 & 0.016 \\ \hline 27 & 0.029 \\ \hline 6 & 3.0 \\ \hline 5 & 1.2 \\ \hline .7 & 11.6 \\ \hline .4 & 97.5 \\ \hline .7 & 99.5 \\ \hline .1 & 91.2 \\ \hline .00 & 100.0 \\ \hline 0.0 & 100.0 \\ \hline 0.0 & 100.0 \\ \hline 0.0 & 100.0 \\ \hline \end{array}$	99.5
	M_2	91.1		88.1
	EWOC-POM	100.0	100.0	100.0
Percent of trial with estimated MTD within 0.10 of γ	M_1	100.0	100.0	100.0
	M_2	100.0	100.0	100.0

Table 2: Summary statistics for trial safety and efficiency under model misspecification when the true MTD $\gamma = 0.1$. Rows 2–6 give the summary statistics based on all patients from all 1000 trials.

the absence of DLT. Specifically, if the current patient experiences drug-related grade 2 toxicity at the most, then it is ethical not to escalate the dose for the next patient by the same amount as the one had the current patient experienced a maximum of grade 0 or 1 toxicity. The method termed EWOC-POM is an extension of EWOC by accommodating an intermediate grade 2 toxicity to the model. We used a proportional odds model to describe the dose-toxicities relationship for simplicity. We proved that if the maximum grade of toxicity experienced by patient k - 1 within one cycle of therapy is grade 2, then the dose allocated to patient k is lower than the dose that would have been given to patient k had the maximum grade of toxicity experienced by patient k - 1 been grade 0 or 1. Furthermore, we also showed that the coherence properties of EWOC are maintained.

We studied design operating characteristics by simulating a large number of trials under different scenarios of the dose-toxicity relationships. EWOC-POM was compared to EWOC with respect to the primary goals of cancer phase I trials, safety and efficiency of the estimate of the MTD. We found that in general, the safety of the trial is not compromised when we account for an intermediate grade 2 toxicity. In particular, when the unknown MTD is close to the initial dose, a substantial number of patients are overdosed when using EWOC relative to EWOC-POM, and if the current patient experiences grade 2 toxicity, then the next patient is more likely to be overdosed using EWOC compared to EWOC-POM. The loss in efficiency of the estimate of the MTD by introducing an extra parameter to the model is very marginal as was shown by the simulation results of the various scenarios. We also showed that the proportional odds assumption is robust to model misspecification when the true MTD is close to the minimum dose. However, the bias of the estimate of the MTD increases as a function of the MTD under model misspecification. In any case, safety of the trial as assessed by the number of patients exhibiting DLT and number of patients that are overdosed was never compromised.

We have shown that Theorem 3.1 holds under the proportional odds assumption using EWOC scheme with link functions satisfying monotonicity conditions as a function of the MTD. One can easily prove that a similar ethical constraint stated in Theorem 3.1 can be established using the Bayesian CRM originally proposed in O'Quigley et al. [3]. In fact, a more general theorem can be established for a Bayes estimate using a general convex loss function. Extensions of EWOC-POM to accommodate patients' baseline characteristics ([30]) and time to event DLT for late onset toxicities are being investigated. In conclusion, EWOC-POM is a good alternative design to EWOC if clinicians expect to see a substantial number of grade 2 toxicities induced by the agent or drug combinations under study.

Appendix

Proof of Theorem 3.1. To simplify notation and presentation of the proof, we assume that $X_{\min} = 0, \rho_0 \le \rho_1$ are fixed, and let us drop the nuisance parameters ρ_0 and ρ_1 from $F_1(\rho_0, \rho_1, \gamma; x)$, and $F_2(\rho_0, \rho_1, \gamma; x)$. Let $L_k(\gamma) = L_k(\rho_0, \rho_1, \gamma \mid D_k)$, and $\pi(\gamma)$ be a proper prior density for γ . If $Y_k = 0, L_k(\gamma) = L_{k-1}(\gamma)[1 - F_1(\gamma; x_k)]$, and if $Y_k = 1, L_k(\gamma) = L_{k-1}(\gamma)[F_1(\gamma; x_k) - F_2(\gamma; x_k)]$. Using Bayes' rule,

$$\begin{split} \prod_{k} (t;0) &- \prod_{k} (t;1) \\ &= \frac{\int_{0}^{t} L_{k-1}(\gamma) \left[1 - F_{1}(\gamma;x_{k})\right] \pi(\gamma) d\gamma}{\int_{0}^{t} L_{k-1}(\gamma) \left[F_{1}(\gamma;x_{k}) - F_{2}(\gamma;x_{k})\right] \pi(\gamma) d\gamma} \\ &= A^{-1} \left[\int_{0}^{t} \int_{0}^{1} L_{k-1}(\gamma) L_{k-1}(\gamma') \pi(\gamma) \pi(\gamma') \pi(\gamma') \left[1 - F_{1}(\gamma;x_{k})\right] \left[F_{1}(\gamma';x_{k}) - F_{2}(\gamma';x_{k})\right] d\gamma' d\gamma\right] \\ &- A^{-1} \left[\int_{0}^{t} \int_{0}^{1} L_{k-1}(\gamma) L_{k-1}(\gamma') \pi(\gamma) \pi(\gamma') \left[F_{1}(\gamma;x_{k}) - F_{2}(\gamma;x_{k})\right] \left[1 - F_{1}(\gamma';x_{k})\right] d\gamma' d\gamma\right] \\ &= A^{-1} \left[\int_{0}^{t} \int_{0}^{1} L_{k-1}(\gamma) L_{k-1}(\gamma') \pi(\gamma) \pi(\gamma') \left[F_{1}(\gamma;x_{k}) - F_{2}(\gamma;x_{k})\right] \left[1 - F_{1}(\gamma';x_{k})\right] d\gamma' d\gamma\right] \\ &= A^{-1} \left[\int_{0}^{t} \int_{0}^{1} L_{k-1}(\gamma) L_{k-1}(\gamma') \pi(\gamma) \pi(\gamma') \left[1 - F_{1}(\gamma;x_{k})\right] \left[F_{1}(\gamma';x_{k}) - F_{2}(\gamma';x_{k})\right] d\gamma' d\gamma\right] \\ &- A^{-1} \left[\int_{0}^{t} \int_{0}^{1} L_{k-1}(\gamma) L_{k-1}(\gamma') \pi(\gamma) \pi(\gamma') \left[F_{1}(\gamma;x_{k}) - F_{2}(\gamma;x_{k})\right] \left[1 - F_{1}(\gamma';x_{k})\right] d\gamma' d\gamma\right] \\ &= A^{-1} \left[\int_{0}^{t} \int_{t}^{1} L_{k-1}(\gamma) L_{k-1}(\gamma') \pi(\gamma) \pi(\gamma') \left[F_{1}(\gamma;x_{k}) - F_{2}(\gamma;x_{k})\right] \left[1 - F_{1}(\gamma';x_{k})\right] d\gamma' d\gamma\right] \\ &= \left[F_{1}(\gamma;x_{k}) - F_{2}(\gamma;x_{k})\right] \left[1 - F_{1}(\gamma';x_{k})\right] \left[F_{1}(\gamma';x_{k}) - F_{2}(\gamma';x_{k})\right] d\gamma' d\gamma\right] \\ &- \left[F_{1}(\gamma;x_{k}) - F_{2}(\gamma;x_{k})\right] \left[1 - F_{1}(\gamma';x_{k})\right] \left[F_{1}(\gamma';x_{k}) - F_{2}(\gamma';x_{k})\right] d\gamma' d\gamma\right],$$
(A.1)

where

$$A = \iint_{0}^{1} L_{k-1}(\gamma) L_{k-1}(\gamma') \left[1 - F_{1}(\gamma; x_{k}) \right] \left[F_{1}(\gamma'; x_{k}) - F_{2}(\gamma'; x_{k}) \right] \pi(\gamma) \pi(\gamma') d\gamma' d\gamma.$$
(A.2)

Since $\gamma \leq \gamma'$ and $(F_1 - F_2)/(1 - F_1)$ is monotonically decreasing in γ , then $[F_1(\gamma'; x_k) - F_2(\gamma'; x_k)]/[1 - F_1(\gamma'; x_k)] \leq [F_1(\gamma; x_k) - F_2(\gamma; x_k)]/[1 - F_1(\gamma; x_k)]$, which implies that $[1 - F_1(\gamma; x_k)][F_1(\gamma'; x_k) - F_2(\gamma'; x_k)] \leq [F_1(\gamma; x_k) - F_2(\gamma; x_k)][1 - F_1(\gamma'; x_k)]$. Hence, $\Pi_k(t; 0) \leq \Pi_k(t; 1)$, which implies that $\Pi_k^{-1}(\alpha; 0) \geq \Pi_k^{-1}(\alpha; 1)$, that is, $x_{k+1} \geq x'_{k+1}$. This completes the proof of Theorem 3.1.

Proof of Theorem 3.2. Using the notation in the proof of Theorem 3.1, if $Y_k = 0$, then $L_k(\gamma) = L_{k-1}(\gamma)[1 - F_1(\gamma; x_k)]$, and if $Y_k = 2$, then $L_k(\gamma) = L_{k-1}(\gamma)F_2(\gamma; x_k)$. Since both F_1 and F_2 are monotonically decreasing in γ , then the result of the theorem follows from the proof of Theorem 1 in Tighiouart and Rogatko [23].

WinBUGS Code

Assume that the toxicity response *Y* has 3 categories:

Y = 1 if patient has grade 0 or 1 toxicity

Y = 2 if patient has a grade 2 toxicity

Y = 3 if patient has grade 3 or 4 toxicity, that is, DLT

Dose is standardized between 0 and 1.

model {

for (i in 1:N) {

Likelihood

 $logit(eta[i,1]) <- (logit(rho1)) - (1/mtd)^*(logit(theta) - logit(rho0))^*X[i]$

 $logit(eta[i,3]) <- logit(rho0) + (1/mtd)^*(logit(theta) - logit(rho0))^*X[i]$

rho1 = P(grade 2 or more toxicity at initial dose)

rho0 = P(DLT or grade 3 or 4 toxicity at initial dose)

MTD = dose producing DLT in theta fraction of the population

```
for (i in 1:N) {
    p[i,1] <-eta[i,1]
    p[i,3] <-eta[i,3]
    p[i,2] <-1-(eta[i,1]+eta[i,3])
    Y[i]~dcat(p[i,])
    }
# Prior Distributions
rho0 ~ dunif(0, theta)
rho1 ~ dunif(rho0, 1)</pre>
```

```
mtd ~ dunif(0,1)

}

# Data

list(Y = c(1, 2, 2, 2, 3, 1, 2, 3, 3, 1, 2, 2, 1, 3),dose =

c(0.1, 0.3262, 0.3873, 0.4390, 0.4892, 0.3810, 0.4298, 0.4681, 0.3980,

0.3339, 0.3650, 0.3788, 0.3986, 0.4308, theta = 0.333333333, N = 14)

# Initial values

list(rho0 = 0.05, rho1 = 0.15, mtd = 0.3).
```

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